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Magnetic scaffold for drug targeting: evaluation of cephalosporins controlled release profile**Dan Eduard Mihaiescu¹, Alexandru Mihai Grumezescu^{1*}, Paul Catalin Balaure¹,
Diana Elena Mogosanu¹, Vanessa Traistaru¹****ABSTRACT**

The great problem associated with drug administration is the inability to target a specific area of the body. To reach an acceptable therapeutic level, large doses of the drug must be administered. Only a part of the dose will actually reach the intended disease. Magnetic targeting simplifies drug administration procedures, increases the concentration of the drug at target sites and decreases the concentration of the drug at non-target sites. This study was focused to evaluate the controlled release profile of cephalosporins from magnetic diethylaminoethyl-cellulose hybrid material (magnetic scaffold). Dissolution behavior of these magnetic scaffolds was evaluated using a modified HPLC system. It was found that in all cases, at large time values, the cephalosporin's concentration was much below the solubility plateau for the pure active compound, demonstrating that the adsorption on the surface of magnetic scaffolds is a valuable procedure to attain controlled release.

Keywords: *magnetic drug targeting, drug delivery, cephalosporins, hybrid materials, cellulose, magnetic scaffolds*

1. Introduction

The idea behind magnetic drug targeting is that magnetic drug carrier (nano)particles [1,2] can be attracted to and retained at a specific site in the body using an external magnetic field source [3]. Magnetic drug targeting is unique in that it represents not just one specific area, but a variety of disciplines ranging from basic materials science to bioscience [4]. The development of hybrid materials [5], nanostructures [6], metal nanoparticles [7,8,9] or nanocomposites [10,11,12] for the delivery of therapeutic agents [13] has introduced new opportunities for the improvement of medical treatment [14] and drug delivery [15]. Magnetic nanoparticles [16,17] have an important application such as magnetic drug delivery or nano-carriers [18] for the treatment of various types of diseases [19]. There is an increasing interest in inventing new magnetic nanoparticles [20] because of their wide applications [21]. Hybrid nanomaterials exhibit unique electronic, optical, and catalytic properties due to their size, morphology and large surface area [22,23]. Cephalosporins [24] are antibiotics with a structure and activity similar to penicillins [25]. They are resistant to penicillinase, but susceptible to cephalosporinases. They have a large action spectrum, including Gram-positive (*Staphylococcus sp.*, *Streptococcus sp.*, *Corynebacterium diphtheriae*) and Gram-negative (*Neisseria gonorrhoeae*, *Haemophilus influenzae*, *Escherichia coli*, *Proteus sp.*, *Klebsiella sp.*)

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microorganisms. In this context, our aim was to study the controlled release profile of Cephalosporins from magnetic DEAE-Cellulose monitored by HPLC system.

2. Experimental section

2.1. Magnetite/Diethylaminoethyl-Cellulose/Antibiotics: preparation and characterization.

Cephalosporins were chosen from the commercially available class of β -lactams antibiotics: Cefuroxime, Cefotaxime, Cefoperazone, Ceftriaxone, Cefepime. Magnetic scaffold was prepared and characterized according to our previous study, as follows: diethylaminoethyl-cellulose (DEAE-C) was added in aqueous solution of NaOH (2%) and then Fe^{2+} and Fe^{3+} (in 1:2 molar ratio) were dissolved in ultrapure water and were added drop-wise under constant stirring at 25 °C. The DEAE-C/ Fe_3O_4 (magnetic scaffold) was separated by applying a magnetic field, and washed several times with water and then with ethanol. The hybrid materials were finally dried at 50° (DEAE-C₅₀) and 100 °C (DEAE-C₁₀₀). After drying in oven at 50° and 100°C for 24 h, the magnetic magnetic scaffolds were dispersed in minimum quantity of ultra-pure water and then the cephalosporins were added. The mixture was grounded for 10 min. It was dried to 40°C for 6 h. The concentration of deposited cephalosporins was 10 %. Scanning electron micrographs of fibrillated Fe_3O_4 /DEAE-cellulose presented no considerably phenomena about the morphology in comparison with untreated DEAE-cellulose according to our previous study [26]. To point out the deposition of cephalosporins on the surface of magnetic scaffolds, FT-IR spectra were performed. Many peaks in the “fingerprint” region between 1600 and 1200 cm^{-1} were observed, as well as changes in the bands area. The “fingerprint” region of the reference and magnetic scaffolds/cephalosporins spectra shows clear differences after deposition of cephalosporins.

2.2. HPLC release control. The cephalosporin’s controlled release dynamics from the magnetic hybrid material was studied using an Agilent 1100 series high pressure liquid chromatograph. All the reagents used in the experimental work were of analytical grade. HPLC release control were performed with a modified Agilent 1100 series high-performance liquid chromatography (Agilent Technologies, Palo Alto, USA) equipped with quaternary pump, vacuum degasser, UV-VIS detector (Figure 1). Chromatographic software HP ChemStation was used for data collection and processing. The samples were introduced in the working apparatus, thermostated at 25°C, under controlled and continuous stirring. In order to avoid migration of the magnetic hybrid material through the system, the sample (40 mg of hybrid support along with the deposited active compound) was placed in a filter paper sample basket of small porosity. Ultra-pure water was used as mobile phase with a flow rate of 3 mL/min. The obtained results are plotted in Figure 2.

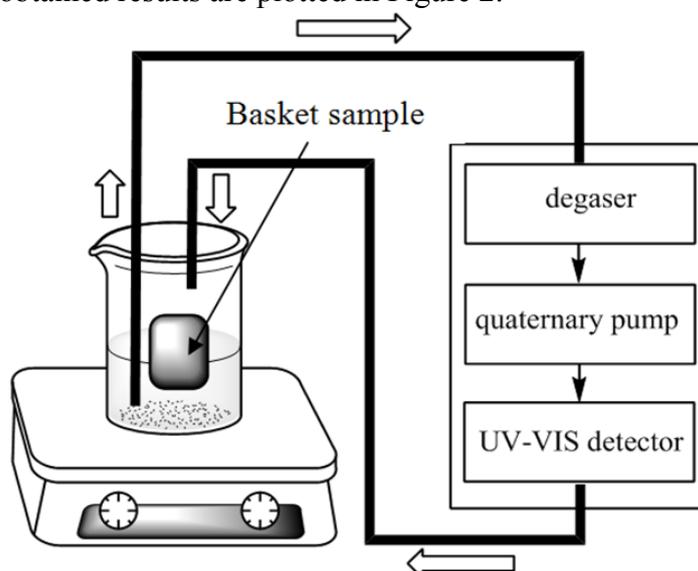


Figure 1: Modified HPLC system for release control

3. Results section

For all studied cephalosporins, the same quantity that was first used to determine the corresponding solubility limit of each compound was subsequently deposited on the magnetic scaffolds (DEAE-C₅₀ and DEAE-C₁₀₀).

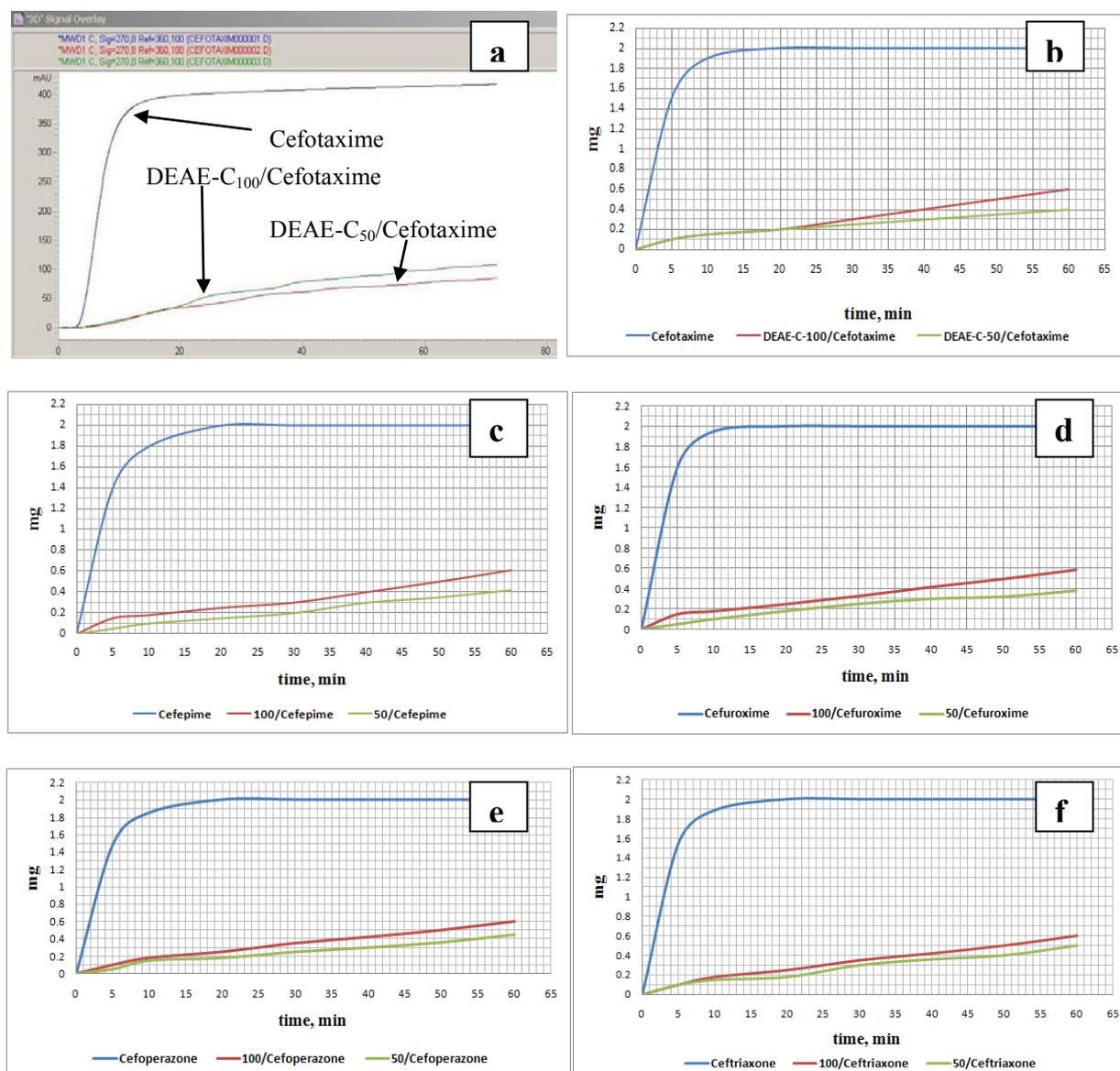


Figure 2: Release control profile of Cephalosporin's: (a) Overlays of HPLC chromatograms of Cefotaxime, Fe₃O₄/DEAE-Celullose₅₀/Cefotaxime and Fe₃O₄/DEAE-Celullose₁₀₀/Cefotaxime; (b) Cefotaxime, (c) Cefepime, (d) Cefuroxime, (e) Cefoperazone, (f) Ceftriaxone: amount of cephalosporin's released from magnetic scaffolds in one hour.

In Figure 2(a) the overlays HPLC chromatogram of pure Cefotaxime, DEAE-C₅₀/Cefotaxime and DEAE-C₁₀₀/Cefotaxime were plotted. It was observed that at times over 1 h the water solubility plateau for the Cefotaxime was not reached, clearly indicating that the cephalosporin is gradually released in aqueous medium from the magnetic scaffold support. In figure 2 (a-f) the quantification of amounts released for all pure cephalosporins, DEAE-C₅₀/Cephalosporins and DEAE-C₁₀₀/Cephalosporins were plotted. In all cases, the maximum pure active compound concentration

was reached after less than 10 min, being followed by a plateau that indicates that the solubility limit corresponding to the complete dissolution of each active compound was attained. The complete release of the active compound from the magnetic materials is expected to reveal a similar concentration-time profile. The controlled release properties of the prepared DEAE-C₅₀ and DEAE-C₁₀₀ were high lightened by the fact that the active compound concentration was much below its solubility limit after 1 h, in every experiment. A period of approximately 10 hours is necessary for the complete release of the active compound from the support. In all experiments, on the mg vs. time curve, two or three distinct regions of different slope were observed. Some changes in the release process can explain the passage from one region to another. Such changes were presumed to be due to the formation of multiple adsorption shells in the synthetic process. Firstly, the solvation process affects the outermost shell and continues with the other multiple adsorption shells. Therefore, the successive release of different adsorption shells starting with the outermost shell of the whole magnetic scaffolds/successive adsorption shells and moving to its interior can explain the appearance of several regions of different slope. Slight changes in the intermolecular forces are concomitant with the successive dissolution of the multiple adsorption shells, the adsorption shell being gradually closer to the outer surface of the magnetite/diethylaminoethyl-cellulose magnetic hybrid materials.

4. Conclusions

The capability of magnetic cellulose hybrid material for local delivery of antibiotics increases their utility in biomedical applications. The drugs were successfully incorporated and released from micro fibrous scaffolds without structural integrity loss or change in functionality according to our previous study [26]. The *in vitro* drug release properties of both magnetic scaffolds were investigated. It was observed that the cephalosporins loaded onto magnetic scaffolds presented a slow initial burst during the first 5 minutes followed by a rather constant and low release profile over the subsequent period of 55 minutes. The cephalosporins without magnetic scaffolds showed a sharp initial burst during the first 5 minutes. The whole release period of pure cephalosporins could last up to 10 minutes, in comparison with the magnetic scaffolds drugs that even after 1 hour did not reach the maximum release. At high levels of magnetic scaffold dehydration, the drug interaction with the support is weaker. These distinct behaviors make the hybrid structure material promising for new drug release materials.

5. References

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