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Custom Fluorescence Imaging System Exploiting Hyperspectral Camera to Characterize and Diagnose RNA Breast Cancer

Mohamed Aref ^{1,*}, Abou-Bakr M. Youssef ², Abdallah Abdelkader Hussein ³, Sara Abd El-ghaffar ⁴, Yasser H. El-Sharkawy ⁵

- ¹ Biomedical Engineering Researcher, Egyptian Armed Forces, Cairo, EGYPT; Mh-aref@ieee.org (M.A.);
- ² System & Biomedical Engineering Department, Cairo University, Giza, Egypt, aboubakryoussef51@gmail.com (A.B.M.Y.);
- ³ Histopathology department, "Kobri El- Koba" Complex Hospital, Egyptian Armed Forces, Cairo, Egypt, abdallahabdelkaderhussein@gmail.com (A.A.H.);
- ⁴ Radiology Department, Maadi Armed Forces Medical Compound, Cairo, EGYPT, saraabdelghaffar_rabee3@yahoo.com (S.A.E.-g.);
- ⁵ Head of Postgraduate Studies Affairs, Military Technical College, Cairo, Egypt, yhmelsharkawy@mtc.edu.eg (Y.H.E.-S.);
- * Correspondence: Mh-aref@ieee.org (M.A.);

Scopus Author ID: 57217856566

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Abstract: Early diagnosis of breast malignancy is a challenging task to permit this cancer. RNA offers incredible potential as a biomarker for malignant growth because of its noteworthy blood dependability and characteristic articulation in various diseases. We explored the total RNA to select the optimum spectral signature concerning entire blood that could segregate between liver cancer (HCC), early breast cancer growth, and normal persons. A custom Hyperspectral Imaging (HSI) system comprises a hyperspectral camera that works in wavelength (380~1050 nm) with ultraviolet (UV) source light (20 mW, 395 nm). It is associated with the custom software system to measure the total RNA signature of (n=50) subjects (n=10 HCC patients, n=15 breast cancer, and n=25 normal persons as a control). Theexperimental result shows that the scattering absorption of all the investigated samples is high at 395 nm based on (size, shape, medical state). Breast cancer RNA demonstrates fluorescence emission at 431 nm and 493 nm and Phosphorescence at 768 nm compared to the normal and HCC patients. Verifying the experimental results with the RNA cuvette spectral images shows that we could discriminate the HCC from the normal total RNA at 431 nm and the breast cancer from both normal and HCC at 768 nm. This prospective investigation shows that the mutation of the total RNA regarding certain diseases affecting its spectral signature exhibits potential detection of breast tumor and HCC in tissues using extracted RNA from Blood in advance and subsequently surgery in subjects with initialstage breast cancer. A wavelength of 431 nm was optimum for discrimination between the HCC and the normal total RNA, and a wavelength of 768 nm was ideal for breast cancer discrimination.

Keywords: breast malignancy; liquid biopsy; Hyperspectral Imaging System; RNA detection; liver cancer; optical spectroscopy.

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1. Introduction

Breast malignancy is one of the most widely recognized cancers in women worldwide, representing around 570,000 death During the past five years [1,2]. In addition, more than 1.5

million women are identified with malignant breast growth consistently all through the world [3,4]. Breast malignant is a metastatic tumor growth and can generally move to inaccessible organs like the liver, brain, bone, and lung, representing its seriousness [5].

Breast cancer early diagnostic could improve the therapeutic chance and increase the survival rates [6]. Mammography is used widely, which is considered the gold standard of breast cancer screening [7–9]. Other methods, such as Breast Magnetic Resonance Imaging (BMRI) [10,11], Breast Ultrasound (US) [12–14], Tomosynthesis Mammography (3D) [15], Automated Breast US (ABUS) [16–18], and Color Doppler [19–21].

Breast malignant generally start from the ductal hyperproliferation and afterward form into benign cancers or even metastatic carcinomas after continual incitement by different cancer-causing factors [22]. Several genes and receptors are associated with breast cancer, such as (BRCA1, BRCA2, PIK3CA, ESR1, AKT1, ERBB2, HER2, and estrogen receptors). Where mutations and abnormalities increase for together oncogenes and anti-oncogenes assume key parts in the cycles of tumor inception and movement [23–25].

DNA (Deoxyribonucleic acid) and RNA (Ribonucleic-acid) supply and relocate genetic information in living organisms, where DNA: the main component of the nucleus/secure demonstration of complete genetic makeup organism, RNA: exist in the cytoplasm and nucleus/key to data stream inside a cell [26,27].

DNA sequencing has been a backbone of life science innovative work. Although 1990 was the beginning of the launch of the human genome project, next in 1995 was the first bacterium sequencing (influenza). Later, the cancer genome atlas in 2012 published exome sequences from 507 breast cancer [28]. During the previous few years, scientific studies have exhibited the capacity to dependably recognize and evaluate circulating cell-free malignant growth DNA and RNA, for the most part in patients with metastatic sickness [29,30].

DNA and RNA quantification is commonly signified to the same extent as nucleic acid quantification to conclude the mean concentration of the DNA or RNA. Additionally, Sample purity is a significant thought to precisely figure the measure in a sample of DNA or RNA [31,32]. There are two common methods to quantify the DNA or RNA [33].

1.1. The Photometry Ultraviolet-Visible measurement (UV-Vis).

This method is based on a measurement of nucleic acids (DNA and RNA) absorption. The measured light reached the detector afterward passing through the investigated sample is measured concerning incident light. However, the standard UV-Vis absorption spectrum displays a high peak at 260 nm. The schematic Diagram of the Photometry (UV-Vis) and the ideal absorption spectrum are more illustrated in Figure A1 in the appendix. Although, one of the features of this system (simple, no sample preparation with dyes or standards, and could measure purity ratios directly). On the other hand, the disadvantages of this method (cannot differentiate between DNA or RNA, and provide limited sensitivity).

1.2. The Fluorescence measurement.

The fluorometric method for nucleic acids relies on fluorogenic dyes, which combine precisely with DNA or RNA. The signal is calculated by fluorometers by sample excitation with a precise wavelength. Where the schematic Diagram of the fluorescence RNA/DNA quantification demonstrating the optical measurement theory with typically measured Fluorescence signal is displayed in Figure A2 in the appendix. However, the advantages of this

system (precise measurement "DNA, ds DNA, ssDNA, and RNA", sensitive as it could measure pg/mL, accurate despite nucleic acid contaminants). Conversely, the disadvantages of this method (It consumes a lot of time during the test for reagent and sample preparation and it does not provide the purity's information).

Cellular "total" RNA: contains messenger RNA (mRNA) representing (1~5 %) which functions as a template for protein synthesis, Ribosomal RNA (rRNA) representing (≥ 80 %) provides the structural component of ribosomes, Transfer RNA (tRNA) representing (10~15 %) which translates mRNA data into the proper amino acid, where total RNA could be extracted from biological samples by either "Organic extraction" or "Affinity purification" to isolating RNA from the other cellular components [34,35].

The fluorescence process is a result of an interaction that happens when certain atoms called fluorophores or fluorescent dyes absorb light. The assimilation of light by a populace of these particles raises their energy level to a concise, energized state. The theory is more explained in the "Jablonski diagram", as displayed in Figure A3 in the appendix [36]. The Jablonski diagram introduces the light absorption, the vibrational relaxation energy as "Fluorescence", the intersystem crossing process as "Phosphorescence", and the spontaneous low-intensity transition as "Delayed Fluorescence" [37,38].

Hyperspectral imaging (HSI) is a fast progressing and non-invasive imaging method with vast capability for clinical applications. HSI had been exploited in head and neck tumor detection [39]. In the *ex-vivo* breast malignant detection [40–42]. In Prostate tumor detection [43]. Monitoring of the Liver thermal ablation [44–46]. Furthermore, exploiting the HSI in observing radiofrequency ablation [47] and laser ablation therapy exploited for minimum invasive liver tumor exclusion [48]. Additionally, in the measurement of oxygen saturation in the blood and spectral blood vessel delineation [49,50].

In the proposed investigation, we measured the spectral signature of the total RNA mutation in plasma of liver cancer (HCC) and breast cancer patients and in healthy persons as controls, where all measurements are label-free (without anybody injection). We also examined the Fluorescence and side scattering signatures for these cases. Furthermore, we could segregate between the total RNA of the breast cancer concerning the healthy and the HCC investigated samples exploiting HSI capabilities to measure the breast cancer Fluorescence signature.

2. Materials and Methods

2.1. The presented approach interconnections processes.

- Sample preparation from the liquid biopsy (blood).
- > Hyperspectral (HS) scan Images of the investigated samples.
- > The measurements of sample Fluorescence and side scattering signature.
- \triangleright Applying the Custom algorithm.

2.2. The breast cancer detection exploiting optical imaging system.

The system incorporated a hyperspectral (HS) camera, UV light source, and image processing algorithm (normalization, moving average filter to remove the unwanted noise) were exploited as channels to detect the breast cancer fluorescence signature from a liquid biopsy. To attain the necessary HSI records, we utilized the HS camera (Surface Optics, SOC710, USA) with 5 nm spectral resolution, 128 spectral channels, and a push broom. The https://biointerfaceresearch.com/

camera is integrated with a lens (Schneider, 1.9/35, Range 400~1000 nm, Germany). The utilized source light assembly for the HS image scan (THORLABS UV source, 50 mW, USA) with wavelength (395 nm).

The capturing time for each image is about $5 \sim 12$ sec and calculation time is 10-15 sec using DADiSP/SE software (DSP Development Corporation,6.7 student edition, 2020, USA) on a personal laptop (DELL, Intel-core i7,1.8GHz,16 GB RAM, USA), the system Schematic Diagram illustrated in Figure 1.



Figure 1. The Schematic Diagram for the investigated System, (1) The Incorporating UV light source (50 mW,395 nm), (2) The Investigated Sample for the total RNA, (3) The exploited Hyperspectral camera (Surface Optics, SOC710, USA), (4) The Computer and the Image Processing Algorithm.

2.3. Design of the study.

The experimental study design was conducted during the period from October 2019 to February 2020 at "Kobri El Koba Military Complex Hospital". The study was ethically approved by the Institutional Ethical Committee of the "Faculty of Medicine, Ain Shams University, Egypt (No: P.T.REC/009/003156)" and followed the Declaration of Helsinki Ethical Principles for Medicinal Research Comprising Human Subjects. All patients read and signed two copies of a consent form before the beginning of data collection.

2.4. Subject and sample preparation.

We extracted the total RNA from fresh human blood of (n=50) subjects who agreed to participate in the experiment (n= 10 HCC patients, n= 15 breast cancer, and n=25 normal persons as a control). We exploited Mini Kit (Geneoid, RB050/100/300, Taiwan) [51]. We utilized the whole Blood sample Volume (300 μ l) for each participated subject. Exploiting RBC Lysis Buffer (Cleansers and chaotropic salt) from the identified kit to lyse cells and deactivate RNase, the RNA was attached by the glass fiber matrix (membrane optimized for total RNA extraction), while contaminants remain suspended. Next, remove the contaminants with wash buffer while the RNA remains bound to the membrane. Finally, the total RNA is

eluted by RNase-free water and ready for the experimental investigation measurements. The sample preparation is more clarified in Figure 2.



Figure 2. The sample Preparation to Extract the Total RNA; (a) Blood Sample withdrawal from the Participated Investigated Subjects; (b) The Fresh Blood Bag of the Investigated Subjects; (c) The Total RNA Extraction Process, (1) The whole Blood sample Volume (300 µl), (2) Cleansers and chaotropic salt are exploited to lyse cells and deactivate RNase, (3) The RNA is attached by the glass fiber matrix while contaminants remain suspended, (4) Removing of the contaminants with wash buffer while the RNA remains bound to the membrane, (5) The total RNA is eluted by RNase-free Water and ready for the experimental investigations.

2.5. Custom Image Algorithm.

An essential enhancement in HSI and in-advance of image acquisition is a level field correction for data normalization. A highly reflected board (white) and a low reflected board (dark) were exploited to attain relative reflectance from the inspected sample [52]. The dark cube was detained by closing the HS camera cap. Data from a dark image and white equilibrium assessments were used to address the intentional material picture. The important objective of this alteration is to remove impacts on the inspected tissue, as presented in equation (1):

$$RF(\vartheta) = \frac{Ip(\vartheta) - I\beta(\vartheta)}{Iw(\vartheta) - I\beta(\vartheta)} \times 100\%$$
(1)

where RF(ϑ) is the reflectance of the inspected sample image, Ip(ϑ) is the caught picture, I $\beta(\vartheta)$ is the dark captured image with a closing lens, and Iw(ϑ) is the acquired whiteboard picture.

Occupying Data-normalization on the acquired image to remove the unnecessary interference. The initially captured images vary because of the incident light and temperature divergences; spectral images must be normalized involving pixel normalization, as illustrated in equation (2).

$$I_{new} = (I_{previous} - min_{previous}) \frac{max_{new} - min_{new}}{max_{previous} - max_{previous}} + min_{new} \quad (2)$$

Although, normalization modifies an m-dimensional grayscale successive image $I_{previous}$: {A} with intensity estimations in the range $(min_{previous})$ to the extreme

 $(max_{previous})$ into a different image I_{new} : {A} with intensity ratios at the minimum range (min_{new}) to the extreme (max_{new}) . Then, employing the Moving average filter as a filter at kernel value=10 for noise eradication and image enhancement [53], as clarified in equation (3).

$$f(x \times y) = \frac{1}{qt} + \sum_{(r \times c) \in W}^{\infty} S(r \times c)$$
(3)

Where 'S' is the noisy picture, $f(x \times y)$ is the restored picture, and 'r' and 'c' for the row and column coordinates correspondingly, within a window 'W' of size ' $q \times t$ ' where the procedure takes place.

In the presented prospective study, we investigated the total RNA of (n=50) participating subjects (n= 10 HCC patients, n= 15 breast cancer, and n=25 normal persons as a control), where the hyperspectral camera works in a wavelength (380~1050 nm) with ultraviolet (UV) as source light at a wavelength (395 nm). We measured the diffuse reflectance and the fluorescence signature of all the samples to select the optimum spectral signature which could segregate between liver cancer (HCC), early breast cancer growth, and normal persons.

3. Results and Discussion

Concerning the system interconnections techniques and processes, they are preliminary from hyperspectral image scanning for the inspected samples and applying the custom image processing to measure the spectral signatures (diffuse reflectance / Fluorescence / Phosphorescence) of the investigated samples (Normal subject / HCC Patient / Breast Cancer Patient).

Although, we noticed from the measured 1-D spectral signature that the investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) are high absorption at the wavelength (395 nm) based on (size, shape, previous medical history, recent medical state) for each case concerning the ultraviolet (UV) source light (20 mW, 395 nm). However, the Total RNA Spectral Signature of the Breast Cancer (in the green dotted line) Demonstrates Emission at 431 nm and 493 nm and Phosphorescence at 768 nm concerning the Normal (solid blue line) and HCC patients (Red dotted line), as shown in Figure 3.

We used the measured 1-D spectral signature to select the optimum spectral images to apply the custom image processing and verify the experimental results with the RNA cuvette spectral images. Consequently, we apply the custom image processing on the acquired scanned cube images for each type of investigated sample separately to validate the hypothesis regarding the spectral signatures.

Initially, we examined the normal control total RNA samples and we used the measured 1-D spectral signature as guidance to select the optimum spectral images at the selected wavelengths (395 nm, 431 nm, 493 nm, and 768 nm). Where the complete worksheet for the scanned normal control total RNA samples demonstrating the spectral images at each wavelength, then the applied custom image processing is displayed in Figure A4 in the appendix.

Even though the scanned Cube image for the normal control total RNA samples shows high absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), as shown in Figure 4-a, on the other hand, the sample did not glow or represent any emissions at a wavelength (431 nm), as displayed in Figure 4-b. Subsequently, the sample provides high emission at a wavelength (493 nm) and almost vanished with no emission at a wavelength (768 nm), as demonstrated in Figure 4-c and Figure 4-d, respectively.



Figure 3. The Spectral Signature of Three of the Investigated Samples (Normal subject / HCC Patient / Breast Cancer Patient) Identifying the High Absorption of the whole Samples at a wavelength (395 nm) regarding the Ultraviolet (UV) source light (20 mW, 395 nm), where the Total RNA Spectral Signature of the Breast Cancer (dotted green line) Demonstrates Emission at 431 nm and 493 nm and Phosphorescence at 768 nm with respect to the Normal (solid blue line) and HCC patients (Red dotted line).



Figure 4. The worksheet window of the scanned Cube image for the normal control total RNA samples exploiting the proposed hypothesis for the spectral signature images after applying the custom image processing; (a) The sample was highly absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), (b) The sample did not glow or represent any emissions at a wavelength (431 nm), (c) The sample provides high emission at a wavelength (493 nm), (d) The sample is almost disappeared with no emission at a wavelength (768 nm).

Next, we investigated the HCC samples and applied the same previous procedures done with the normal control total RNA samples by selecting the spectral images at the wavelengths (395 nm, 431 nm, 493 nm, and 768 nm) with respect to the measured 1-D spectral signature. The complete worksheet for the scanned HCC total RNA samples demonstrated the spectral

images at each wavelength, and the applied custom image processing is displayed in Figure A5 in the appendix.

Despite the fact, the scanned Cube image for the HCC total RNA samples shows high absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), as shown in Figure 5-a. On the other hand, the sample represents a little bit of emission at a wavelength (431 nm), as displayed in Figure 5-b. Subsequently, the sample provides high emission at a wavelength (493 nm) and almost vanished with no emission at a wavelength (768 nm), as demonstrated in Figure 5-c and Figure 5-d, respectively.



Figure 5. The worksheet window of the scanned Cube image for the HCC total RNA samples exploiting the proposed hypothesis for the spectral signature images after applying the custom image processing; (a) The sample was highly absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), (b) The sample represents a little bit emission at a wavelength (431 nm), (c) The sample provides high emission at a wavelength (493 nm), (d) The sample is almost disappeared with no emission at a wavelength (768 nm).



Figure 6. The worksheet window of the scanned Cube image for the Breast Cancer total RNA samples exploiting the proposed hypothesis for the spectral signature images after applying the custom image processing; (a) The sample was highly absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), (b) The sample represents a moderate emission at a wavelength (431 nm), (c) The sample provides high emission at a wavelength (493 nm), (d) The sample still representing emission at a wavelength (768 nm).

Furthermore, investigating the breast cancer samples at the selected wavelengths (395 nm, 431 nm, 493 nm, and 768 nm) concerning the measured 1-D spectral signature. Despite the fact, the scanned Cube image for the breast cancer total RNA samples shows high absorption at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), as shown in Figure 5-a. On the other hand, the sample represents a moderate emission at a wavelength (431 nm), as displayed in Figure 5-b. Subsequently, the sample provides high emission at a wavelength (493 nm) and still represents emission at a wavelength (768 nm), as demonstrated in Figure 5-c and Figure 5-d, respectively.



Figure 7. (a) The three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength (395 nm), (b) The three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength (431 nm), (c) The three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength (768 nm).

Finally, for the result validation, we repeat the experiment of the investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at the same time concerning the three different wavelengths (395 nm, 431 nm, 768 nm). At each wavelength (395 nm, 431 nm, 768 nm), we measure each case's emission intensity, as clarified in the entire worksheet in Figure A6, Figure A7, Figure A8 in the appendix, respectively. Figure 7 was constructed from Figure A6-d, Figure A7-d, Figure A8-d in the appendix to highlight the emission variation for each case at the various wavelengths (395 nm, 431 nm, 768 nm).

Breast tumor is the most widespread tumor among women worldwide [54]. The occurrence of breast tumors is recognized to the escalation with age [55,56], essentially due to the mammary glands of bodily mutations [57]. Liable on the various subtypes, early-stage breast tumor is responsive to therapeutic cancer resection surgery. In spite of this, early-stage breast tumor detection is a challenging task. Furthermore, it is vital for decreasing cancer-related mortality [58]. However, its consequence varies with respect to the types and grades of the disease. For breast tumor grade II and III, the tumor development is much faster than grade I. Therefore, the survival and diagnosis could be significantly enhanced with an early diagnostic for the tumor ≤ 2 cm [59].

Breast tumor is frequently divided into several subtypes regarding the tumor's molecular landscape [60,61]. Conventional methods for breast cancer diagnosis, for instance, tissue biopsy, are not inclusive enough to acquire the whole genomic landscape of breast cancers. But, with the institution of novel methods, the relevance of liquid biopsy has been improved with respect to breast cancer management incorporating (cancer early detection, monitoring, the expectation of diagnosis, and response to therapy) [62].

Throughout the formation and development of the initial malignant tumor, numerous components are discharged into the blood resulting in apoptosis and necrosis [63,64]. Some of which incorporate cell-free RNA (RNA_{cf}), circulating tumor cells (CTCs), and circulating tumor DNA (DNA_{ct}). Applications of liquid biopsy have the ability to address the necessity for a customized non-invasive tumor screening system. Consequently, various components of breast cancers in the blood can be employed for more successful diagnosis, expectation prognosis, targeted therapeutic, and detection of resistance development [65].

The proposed system incorporates (side scattering, fluorescence, Phosphorescence) measurements. Where fluorescence phenomena were investigated thru the measurement of the spectral signatures of the investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) with respect to the changes of the optical properties for each sample, this was achieved by exploiting the HSI system with source light UV light (UV, 20 mW, 395 nm).

We observed from the measured 1-D spectral signature of the investigated total RNA samples are highly absorbed in a wavelength (395 nm) with respect to the UV source light (20 mW, 395 nm). The normal cases were displayed in (solid blue line) and HCC patients (Red dotted line), and the Breast Cancer (in the green dotted line). However, the total RNA spectral signature of the breast cancer demonstrates emission at 431 nm and 493 nm and Phosphorescence at 768 nm with respect to the Normal (solid blue line) and HCC patients (Red dotted line), as shown in Figure 3.

We used the measured 1-D spectral signature as guidance to select the optimum spectral images to validate the output result. The scanned cube images for each type of the investigated sample were processed to remove the unnecessary background noise and enhance the images at the selective wavelengths (395 nm, 431 nm, 493 nm, and 768 nm).

We initially examined the normal control total RNA samples spectral images at the selected wavelengths (395 nm, 431 nm, 493 nm, and 768 nm). However, we noticed that for the normal control, total RNA samples show high absorption at a wavelength (395 nm) with respect to the excitation source light (UV, 20 mW, 395 nm), as shown in Figure 4-a. However, the sample did not glow or represent any emissions at the wavelength (431 nm), as displayed in Figure 4-b. Subsequently, the sample provides high emission at the wavelength (493 nm) and almost vanished with no emission at the wavelength (768 nm), as demonstrated in Figure 4-c and Figure 4-d, respectively. Furthermore, the complete worksheet for the normal total RNA samples is more clarified in Figure A4 in the appendix.

Then, we investigate the HCC total RNA samples at the selected wavelengths (395 nm, 431 nm, 493 nm, and 768 nm) with respect to the measured 1-D spectral signature. Despite the fact, the HCC total RNA samples show high absorption at a wavelength (395 nm), as shown in Figure 5-a. On the other hand, the sample represents a little bit of emission at the wavelength (431 nm), as displayed in Figure 5-b. Subsequently, the sample provides high emission at the wavelength (493 nm) and almost vanished with no emission at the wavelength (768 nm), as demonstrated in Figure 5-c and Figure 5-d, respectively. Additionally, the complete worksheet for the HCC total RNA samples is more elucidated in Figure A5 in the appendix.

Furthermore, the breast cancer total RNA samples were investigated at the selected wavelengths (395 nm, 431 nm, 493 nm, and 768 nm). The scanned Cube image for the breast cancer total RNA samples shows high absorption (395 nm) wavelength, as shown in Figure 6a. The sample represents a moderate emission at the wavelength (431 nm), as displayed in Figure 6-b. Consequently, the sample provides high emission at the wavelength (493 nm) and still represents emission at the wavelength (768 nm), as demonstrated in Figure 6-c and Figure 6-d, respectively.

Finally, for data validation, we explored the investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) instantly with respect to the three different wavelengths (395 nm, 431 nm, 768 nm) to highlight the emission variations for each case.

However, Figure A6 in the appendix presents the three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength 395 nm. From Figure A6-e, we calculate the emission intensity for each case at the scanned line 269 Y-axis with values (Normal = 175 A.U, HCC = 90 A.U, Breast cancer = 250 A.U). Then, from Figure A7 in the appendix, we calculate the emission intensity for each case at wavelength 431 nm for the scanned line 269 Y-axis with values (Normal = 165 A.U, HCC = 140 A.U, Breast cancer = 185 A.U). Furthermore, from Figure A8 in the appendix, we calculate the emission intensity for each case at wavelength 768 nm for the scanned line 269 Y-axis with values (Normal = 155 A.U, HCC = 150 A.U, Breast cancer = 210 A.U). Finally, Figure 7 was constructed from Figure A6-d, Figure A7-d, Figure A8-d in the appendix to highlight the emission variation for each case at the various wavelengths (395 nm, 431 nm, 768 nm).

4. Conclusions

A customized optical imaging system incorporating the HS camera has been launched to distinguish between breast cancer and HCC using a particular spectral signature for total RNA with a promising result associated with a respectable accuracy and sensitivity in minimum investigation time. The experimental result shows that all the investigated samples (normal / HCC/ breast cancer) have high absorption at wavelength 395 nm. Breast cancer RNA demonstrates emission at 431 nm, 493 nm, and Phosphorescence at 768 nm compared to the https://biointerfaceresearch.com/

normal and HCC patients. Verifying the experimental results with the RNA cuvette spectral images shows that we could discriminate the HCC from the normal total RNA at 493 nm and the breast cancer from both normal and HCC at 768 nm. In future work, we intend to build a simple and low-cost system to work with a commercially charge-coupled device (CCD) camera to be exploited in cancer (breast cancer / HCC) early detection and infectious syndromes.

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Conflicts of interest

The authors state and declare that there are no conflicts or competing interests. All the coauthors agreed to the publication of this research study

Ethics approval

The experimental study design was conducted from October 2019 to February 2020 at "Kobri El Koba Military Complex Hospital". The study was ethically approved by the Institutional Ethical Committee of the "Faculty of Medicine, Ain Shams University, Egypt (No: P.T.REC/009/003156)" and followed the Declaration of Helsinki Ethical Principles for Medicinal Research Comprising Human Subjects.

Consent to participate

All patients read and signed two copies of a consent form before data collection and within this research study.

Availability of data and material

The authors state and declare that all data exist and are available.

Code availability

The authors state and declare that all code exists and is available.

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Appendix



Figure A1. (a) The schematic Diagram of the Photometry (UV-Vis) demonstrating the optical signal measurement idea for the calculation of the absorption value of the investigated sample, (b) The ideal signal for the intrinsic absorptivity properties of nucleic acids (DNA and RNA) with peak at 260 nm.







Figure A3. The Jablonski diagram introduces that the light absorption provides sufficient energy to provide the necessary excitation for the electron to move from energy level (S_0) to level (S_1) , then due to the vibrational relaxation release equal amount of energy as "Fluorescence" and the intersystem crossing process as "Phosphorescence", and the spontaneous low-intensity transition as "Delayed Fluorescence", the amount of exciting energy and the reasonable time various regarding the type of the material and exploited light.



Figure A4. The worksheet of the spectral images for the investigated normal control total RNA samples; (**a**) The scanned spectral image of the sample at a wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), (**b**) The scanned spectral image of the sample at a wavelength (431 nm) does not represent any emissions or glowing, (**c**) The scanned spectral image of the sample at a wavelength (493 nm) shows high emission, (**d**) The scanned spectral image of the sample at a wavelength (768 nm) is almost disappeared with no emission, (**e**) The collage Image of the scanned samples spectral images at the various wavelengths (395, 431, 493, and 768 nm), (**f**) The collage Image of the scanned samples spectral images after applying the custom

image processing (normalization, Moving average filter) to remove the background noise.



Figure A5. The worksheet of the spectral images for the investigated HCC total RNA samples; (a) The scanned spectral image of the sample at wavelength (395 nm) regarding the excitation source light (UV, 20 mW, 395 nm), (b) The scanned spectral image of the sample at wavelength (431 nm) represents a little bit emission, (c) The scanned spectral image of the sample at wavelength (493 nm) provides high emission, (d) The scanned spectral image of the sample at wavelength (768 nm) is almost vanished with no emission, (e) The collage Image of the scanned samples spectral images at the various wavelengths (395, 431, 493, and 768 nm), (f) The collage Image of the scanned samples spectral images after applying the custom image processing (normalization, Moving average filter) to remove the background noise.



Figure A6. The entire worksheet of the three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength 395 nm; (a) The matrix of the spectral images for the investigated normal total RNA samples at wavelength 395 nm, (b) The matrix of the spectral images for the investigated HCC total RNA samples at wavelength 395 nm, (c) The matrix of the spectral images for the investigated breast cancer total RNA samples at wavelength 395 nm, (d) The collage Image of the scanned samples spectral images after applying the custom image processing (normalization, Moving average filter) to remove the background noise with a scanned line at (269 Y-axis) to monitor the emission intensity for each case, (e) The emission Intensity for the various investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) to highlight the difference for each case, (f) The contour mapping for the emission for the various investigated samples (Normal subject / HCC Patient / Breast Cancer Patient).



Figure A7. The entire worksheet of the three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength 431 nm; (a) The matrix of the spectral images for the investigated normal total RNA samples at wavelength 431 nm, (b) The matrix of the spectral images for the investigated HCC total RNA samples at wavelength 431 nm, (c) The matrix of the spectral images for the investigated breast cancer total

RNA samples at wavelength 431 nm, (d) The collage Image of the scanned samples spectral images after applying the custom image processing (normalization, Moving average filter) to remove the background noise with a scanned line at (269 Y-axis) to monitor the emission intensity for each case, (e) The emission Intensity for the various investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) to highlight the difference for each case.



Figure A8. The entire worksheet of the three investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) at wavelength 768 nm; (**a**) The matrix of the spectral images for the investigated normal total RNA samples at wavelength 768 nm, (**b**) The matrix of the spectral images for the investigated HCC total RNA samples at wavelength 768 nm, (**c**) The matrix of the spectral images for the investigated breast cancer total RNA samples at wavelength 768 nm, (**d**) The collage Image of the scanned samples spectral images after applying the custom image processing (normalization, Moving average filter) to remove the background noise with a scanned line at (269 Y-axis) to monitor the emission intensity for each case, (**e**) The emission Intensity for the various investigated samples (Normal subject / HCC Patient / Breast Cancer Patient) to highlight the difference for each case.