

Review of Biopolymer Composite Through 3D Printing Techniques

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Abstract: Since polymers are so important in our daily lives, 3D printing began with a polymer substrate for creating components. Aside from that, biopolymer composites have become popular due to their environmentally friendly, biodegradable, and biocompatible properties. Despite recent advances in 3D printing of biopolymer composites, this paper reviewed the printing technique of each biopolymer composite, which has a large number of printing techniques such as Fused Deposition Modelling (FDM), Selective Laser Sintering (SLS), Stereolithography (SLA), Ink Jet and others that can be used for biopolymer composite due to mechanical properties findings and application. These biopolymer composites are widely utilized in the biomedical field and are predicted to increase their benefits in this field, as well as FDM, which is the most regularly used 3D printing process.

Keywords: Biopolymer composite; 3D printing; FDM; SLS; SLA; Ink jet

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1. Introduction

The method of quickly generating a system or component representation before its ultimate release or commercialization is referred to as rapid prototyping (RP) and is used to define the process in various industries. To put it another way, the goal is to produce something fast, and the result will either be a prototype or a basic model that will serve as the foundation for further models and, ultimately, the finished product. Additive manufacturing (AM) is the official name for what was once known as rapid prototyping and is often referred to as 3D Printing [1]. This technique has allowed a large deal of design flexibility, creating very complex components, products with a high degree of customization, and efficient waste reduction. The most recent one, known as Industry 4.0, is characterized by the adoption of practices that include the combination of advanced information technology and intelligent production systems. As a result, AM plays an essential part in the development of Industry 4.0 due to its various advantages, including the reduction of wasted time and materials, rapid prototyping, high efficiency, and decentralized production processes [2,3]. Methods of additive manufacturing (AM) have seen remarkable expansion and development in recent years. AM for polymers is an intriguing topic with significant potential for transformational and translational research in various sectors, including the biomedical, aerospace, and electronic industries. Extrusion of material, material jetting, vat polymerization, and powder bed fusion are some of the current technologies for polymer additive manufacturing [4]. Meanwhile, on the topic of the monetization of renewable bioresource materials, researchers have produced

exemplary publications. Biopolymers may be derived from a wide variety of biobased raw materials, the most common of which are starch, cellulose, and biomass from wood. When compared to more traditional forms of plastic, they provide a considerable contribution to reducing the overall carbon impact [5]. Materials that comprise a blend of traditional ceramics, ceramics, or unexpected qualities that are not present in polymers are required to use modern technology in additive manufacturing (AM). The blended materials create new materials by combining two or more components, each of which has desirable attributes, in order to generate the traits and characteristics that are required of the finished product; an example of CaP was determined by their biocompatibility and bioactivity of the material [6-9]. The use of many materials in conjunction with one another to achieve the required qualities of each component may provide new possibilities and problems for additive manufacturing research [10].

2. 3D Printing Method Preparation

Due to their biodegradability and nontoxicity, the biopolymers family is an excellent candidate for fabricating implants and bio-devices that will come into direct contact with the human body. Because of this, there is a significant possibility that the biopolymers will be used in the 3D printing of biobased devices [11]. The method of 3D printing is one in which layers are added one on top of the other, and it can be used to create very complex and specialized devices that vary in size from the macro to the micro-scale. In recent years, additive manufacturing (AM) technology has rapidly advanced in various fields and industrial domains, including biomaterials, pharmaceuticals, medical, aerospace, artworks, smart devices, and other areas [12]. These advancements have been made for both metal and polymer materials. The use of 3D printing technology in tissue engineering, which falls under the umbrella term of bioprinting, has led to a substantial number of noteworthy advances in biomedical implants for bone, blood vessels, tissue, and other anatomical components [13]. This research reviews the comprehensive information methods preparation and their applications.

2.1. Fused Deposition Modelling (FDM).

An FDM system, also known as Fused Filament Fabrication-FFF is an advanced technology that is widely used for printing polymeric materials such as polylactic acid (PLA), acrylic butadiene styrene (ABS), polyethylene terephthalate (PET), Polyhydroxyalkanoate (PHA) nylon, and so on. This technology was developed by Fused Filament Fabrication [14]. In FDM, the thermoplastic filaments are passed through one or more printing nozzles at a temperature higher than the melting point of the filament to build a three-dimensional object using a method known as layer-by-layer deposition. After being placed, the layer underneath it will instantly begin to harden and cool, allowing it to form a connection with the layer that will be put directly on top of it shortly thereafter [15-16]. The inexpensive cost of the printer and the ease with which it may be processed have led to FDM being the technology that is utilized the most out of all the others. However, determining the ideal parameters for polymer printing, such as nozzle temperature, printing speed, and any post-processing factors, may be difficult [17]. Figures 1 and 2 depict the illustration and mechanism of Fused Deposition Modelling.

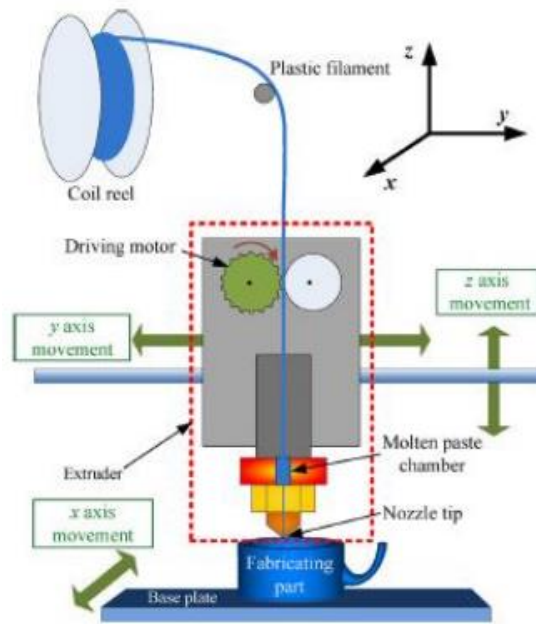


Figure 1. Illustration of fused deposition modeling. Reproduced from [18] with open access from IOP Conf. Ser.: Mater. Sci. Eng. Copyright 2021.

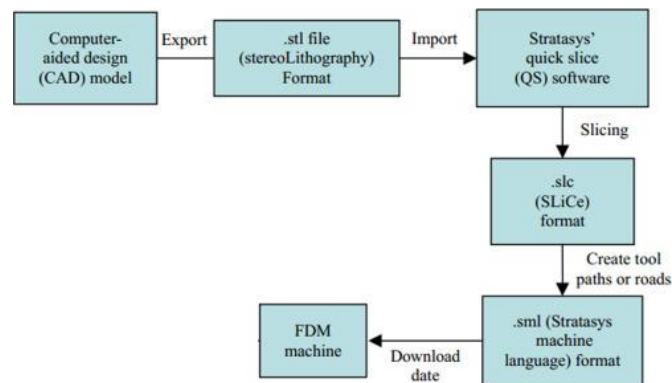


Figure 2. Flowchart of fused deposition modeling. Reproduced from [19] with Elsevier Publishing. Copyright 2020.

Table 1. Overview of biopolymer composites through fused deposition modeling.

References	Material	Printing Technique	Mechanical Properties	Application	Year
[20]	PHA/PF	FDM	Tensile Strength: 10-25MPa	Biomedical	2021
[21]	PHA/SSS	FDM	Tensile Strength: 10-25MPa Young Modulus: 900-1700MPa	Artificial Bone	2018
[22]	PHA/Lignin	FDM	Shear Viscosity: 150.8 Pa.s±15.4Pa.s	Wood Industry	2019
[23]	PHBH/NCF	FDM	Yielding Stress: 17-23MPa Elastic Modulus: 897-1014MPa	N/A	2019
[24]	PLA/PHB/NC	FDM	Storage Modulus: 3-6GPa	Biobased	2020
[25]	PHA/WF	FDM	Tensile Strength: 38.7MPa Flexural Strength: 77.3 MPa	Packaging Industry	2021
[26]	PHBV/RS	FDM	Max. Load: 2N	Piezoelectric Device	2021
[27]	PLA/PHB/Cellulose	FDM	Thermal Stability	Biobased Product	2019
[28]	PCL/Borate Glass	FDM	N/A	Tissue Engineering	2017
[29]	PLA/Graphite	FDM	Young's Modulus: 1866Mpa	Sensors	2020

References	Material	Printing Technique	Mechanical Properties	Application	Year
			Compressive Strength: 38.6MPa		
[30]	PHB/PLA/HA	FDM	Flexural Modulus: 3.20GPa	Biomedical	2022
[31]	PLA/cHA	FDM	Compressive Strength: 2.12MPa	Bone scaffold	2020
[32]	PLGA/TCP	FDM	Compressive Strength: 3.7±0.2MPa Young's Modulus: 114.9±15.4MPa	Bone Scaffold	2022
[33]	PCL/HA	FDM	Tensile Strength: 20.25MPa Flexural Strength: 18.77MPa	Tissue Engineering	2019
[34]	PCL/β-TCP	FDM	Compressive Strength: 20MPa	In vitro	2021
[35]	HDPE/n-HAp	FDM	Plasma Treatment: 399.5eV	Bone Tissue	2022
[36]	PLA/HA/Ch	FDM	Flexural Testing: 120N	Tissue Engineering	2021
[37]	PEEK/cHAp	FDM	Tensile Strength: <50MPa Modulus of Elasticity: 7GPa	Bone Implant	2021
[38]	PCL/PLGA/β-TCP	FDM	Tensile Test: 20MPa	Bone Regeneration	2016
[39]	PLA/Flax Fibre	FDM	Tensile Strength: 10.20MPa	Sustainable Product	2019
[40]	sPEEK/HAP/rGO	FDM	Compressive Strength: 115-135MPa	Bone Implant	2022
[41]	PLA/Ch	FDM	Compressive Strength: 31MPa Tensile Strength: 29MPa Flexural Strength: 37MPa	Scaffold	2020
[42]	PLA/PVC/Wood Powder	FDM	Flexural Strength: 14.14MPa	Scaffold	2022
[43]	PLA/Wood	FDM	Tensile Strength: <35MPa Compressive Strength: <70MPa	Sustainable Filament	2021
[44]	PLA/β-TCP	FDM	Elastic Modulus: 65-72MPa	Scaffold	2021
[45]	PLA/LIPAs	FDM	N/A	Information Storage	2022
[46]	PLA/AV	FDM	N/A	Bone Tissue Engineering	2022
[47]	PLLA/HA/dECM	FDM	Flexural Strength: 150-200MPa	Bone Tissue Engineering	2022
[48]	PLA/CCNF	FDM	Tensile Strength: 23MPa	Dielectric Heat Sources	2020
[49]	PLA/Ti-Zr	FDM	Energy Measurement: 57.0711mW/m ²	Medical Implant	2022
[49]	PLA/Zn	FDM	Compressive Strength: 12-17MPa Elastic Modulus: 500-700MPa	Tissue Regeneration	2022
[50]	PLA/Keratin/Ch	FDM	Elastic Modulus: 1200-1250MPa	Medical Field	2020
[51]	PCL/Gelatin	FDM	Young's Modulus: 12.3±1.6MPa	Tissue Regeneration	2020
[52]	TPU/lignin	FDM	Tensile Strength: 10.87MPa	Biomedical Scaffold	2022
[53]	PLLA/Steel Particle	FDM	Effective Modulus: 0.8-1.5GPa	Tissue Engineering	2018
[54]	Chitin/IC/WC	FDM	N/A	Electrical Energy Delivery	2022
[55]	PLA/DDGS/Plasticizer	FDM	Tensile Strength: 44.9MPa-42.7MPa Young's Modulus: 1565-1500MPa	Sustainable Filament	2021
[56]	PLA/EE	FDM	Tensile Strength: 183MPa	Eco-Friendly Product	2017
[57]	PLA/PP/NFC	FDM	Tensile Strength: 15.2MPa	Structural	2020

References	Material	Printing Technique	Mechanical Properties	Application	Year
			Compressive Strength: 8.5-15.5kN/m Flexural Strength: 142-162kN		
[58]	PLA/Clay	FDM	Modulus Strength: 3.27-3.66GPa Tensile Strength: 46.12-55.58MPa	Sustainable Filament	2018
[59]	PLA/SiC/C	FDM	Recovery Force: 1.75-3.08N	Shape Memory Polymer	2018
[60]	PCL/GNP	FDM	Compressive Strength: 35.3&17.4MPa	Myocardial Tissue Engineering	2022
[61]	PLA/Wood (Poplar Trees)	FDM	Tensile Strength: 50MPa	Renewable Material	2020
[62]	PLA/Rice Husk	FDM	Storage Modulus: 8.6-13.4MPa	Renewable Product	2022
[63]	PLA/WF (Aspen)	FDM	DTG Curved Peak: 330°C	Sustainable Filament	2020
[64]	PLA/AT	FDM	Tensile Strength: 2.6-3.1MPa Young's Modulus: 2.1-2.9GPa	Sustainable Material	2020
[65]	PLA/Ti	FDM	Tensile Strength: 28.3±0.2MPa 40.2±0.2MPa	Scaffold	2020
[66]	PLA/Olive Wood	FDM	E=1.4-2.1GPa Yield Stress: 30.7-40.9MPa	Renewable Material	2022
[67]	PLA/HPMC	FDM	Tensile Strength: 42±3.6MPa	Sustainable Filament	2020
[68]	PLA/Silicon	FDM	Tensile Strength: 60MPa	Sustainable Material	2017
[69]	PHBH/CNCs	FDM	E'=0.1~4.00GPa	Biodegradable Products	2020
[70]	PLA/Almond Shell	FDM	N/A	Sustainable Filament	2022
[71]	PLA/Lignin	FDM	N/A	Healthcare	2019
[72]	PBAT/Wood	FDM	Flexural Strength: 31-53MPa	Pellet	2018
[73]	PLA/Biogenic Carbon	FDM	N/A	Sustainable Filament	2018
[74]	PLA/Hemp	FDM	E'=2333-3130MPa 5.15-7.45MPa	Sustainable Filament	2019
[75]	PCL/ZnHA	FDM	Stiffness Modulus: 37.8MPa	Bone Tissue Engineering	2021
[75]	PCL/ZnHa-rGO	FDM	Stiffness Modulus: 49.5MPa	Bone Tissue Engineering	2021
[76]	PLGA/CQD	FDM	N/A	Scaffold	2022
[77]	PBAT/TiO ₂	FDM	DMA: 3.0±0.2 & 4.3±0.2GPa	Composite Filament	2022
[78]	PCL/Porous Glass	FDM	Compressive Strength: 80±10-102±11MPa	Bone Defect	2019
[79]	PLA/SEBS/CNT	FDM	Tensile Strength: ~3000MPa	Industry	2021
[80]	PLA/Walnut Shell	FDM	Tensile Strength: 2.684MPa	Sustainable Filament	2022
[81]	BioPE/TMP	FDM	N/A	Sustainable Filament	2018
[82]	PHB/MWCNT	FDM	Tensile Strength: 30-35MPa	Sustainable Filament	2021
[83]	PLA/Wood Polysaccharides	FDM	Flexural Modulus: 3.2±0.3GPa	Industry	2018
[84]	PLA-PHB/Corncob	FDM	Tensile Strength: 23MPa Tensile Modulus: 1.4GPa	Sustainable Filament	2022
[85]	MBG/SA	FDM	N/A	Biomedical	2020

2.2. Selective Laser Sintering (SLS).

The additive manufacturing technique known as selective laser sintering (SLS) printing is a kind of powder bed fusion (PBF), which may be used in the production of polymeric components. Based on a previously established CAD model, the laser beam plays a significant part in this process since it is responsible for melting the polymer powder in a selected approach [86]. In this technique, the first layer, which is quite thin, is produced. After that, a new layer is created by simultaneously sintering and heating the material that is already on top of the layer that was created before. This process is done several times until the component has been produced in its entirety [87]. The SLS printing process has a lot of potential to be used in the production of porous scaffolds of a high grade and sophistication that include intricate patterns [88]. This method may also be used in the production of goods containing biopolymer composite such as polyglycolide (PGA), poly lactic-co-glycolic acid (PLGA), Polyether ether ketone (PEEK), etc., which makes them a very good option, and well-tolerated by immune systems and cells [89]. Therefore, 3D printing is a highly ideal and quick manufacturing process that may be employed for the so-called dissolving implants. This is because 3D printing is capable of producing incredibly complex shapes. Figures 3 and 4 show the illustration and mechanism of Selective Laser Sintering, and Table 2 shows its utilization on biopolymer.

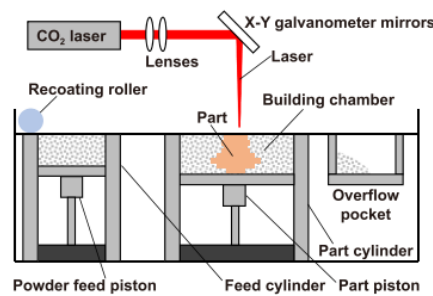


Figure 3. Illustration of selective laser sintering. Reproduced from [90] with open access from Int. J. Extrem. Manuf. Copyright 2022.

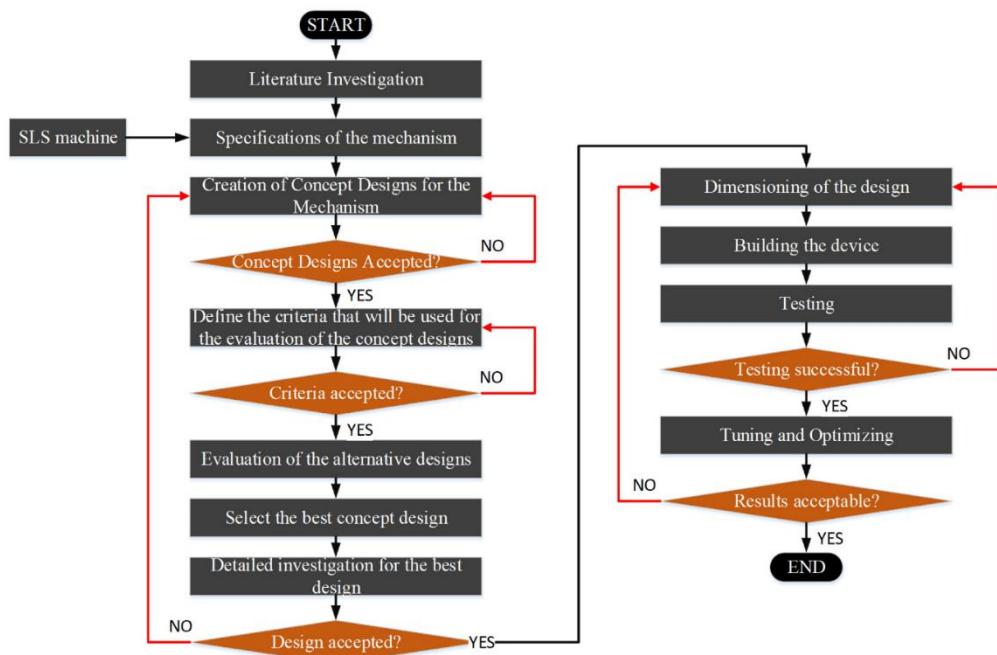


Figure 4. Flowchart of selective laser sintering. Reproduced from [91] with open access from Int. J. Manuf. Mater. Process. Copyright 2022.

Table 2. Overview of biopolymer composite through selective laser sintering.

Reference	Material	Printing Technique	Mechanical Properties	Application	Year
[92]	PHBV/CaP	SLS	Compressive Strength: 0.55MPa	Bone Scaffold	2010
[93]	PLGA/HA	SLS	Compressive Strength: 40MPa	Bone Regeneration	2021
[94]	PEEK/ZrO ₂	SLS	Yield Stress: 5-17MPa	Scaffold	2019
[94]	PEEK/Al ₂ O ₃	SLS	Yield Stress: 28-45MPa	Scaffold	2019
[94]	PEEK/TiO ₂	SLS	Yield Stress: 5-8MPa	Scaffold	2019
[94]	PEEK/Cu	SLS	Yield Stress: 5MPa	Scaffold	2019

2.3. Stereolithography (SLA).

SLA technology is one of the pioneering technologies for 3D printing that uses a photochemical process to enable the manufacture of components or products. This approach may be considered one of the most versatile. An ultraviolet (UV) laser is used in this technology to polymerize the photocurable resin and crosslink the chemical monomers [95]. Therefore, the use of laser irradiation results in the formation of a patterned layer that is two-dimensional. Following the completion of the first phase, the printing platform will shift, allowing for the formation of a subsequent layer. SLA can fabricate the whole product via an iterative process that builds the product layer by layer [96]. SLA has made use of a variety of biopolymers. An aqueous poly(ethylene glycol) (PEG) hydrogel solution, for example, has been prepared, and study results demonstrate that the hydrogel may protect human skin fibroblast cells encapsulated in the solution from injury throughout the SLA process [97]. Figures 5 and 6 illustrate the illustration and mechanism of stereolithography and the utilization of biopolymer composite in Table 3.

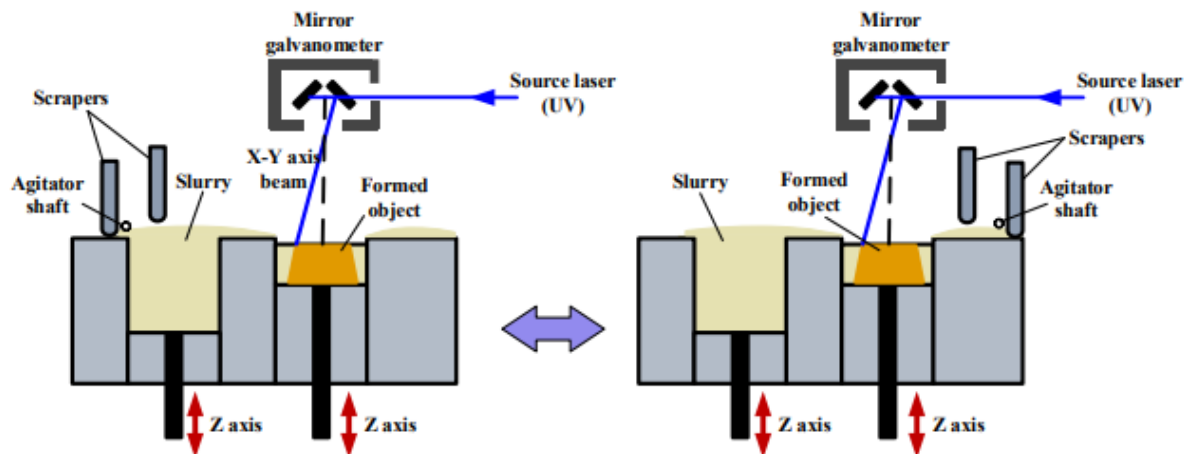


Figure 5. Illustration of stereolithography. Reproduced from [98] with open access from J. Phys.: Conf. Ser. Copyright 2021.

Table 3. Overview of biopolymer composite through stereolithography.

Reference	Material	Printing Technique	Mechanical Properties	Application	Year
[100]	P4HB/PHOH	SLA	N/A	Heart Valve	2002
[101]	45S5 Bioactive Glass	SLA	Tensile Strength: 37.9MPa	Scaffold	2021
[102]	PEGDA/AESO/nHA	SLA	Tensile Strength: 29.81±1.16MPa	Petroleum	2021
[103]	CMC/HA	SLA	N/A	Tissue Engineering	2018
[104]	PLLA/HA	SLA	Max. Strength: 16.6±0.9MPa 155.3±3.3MPa	Bone Scaffold	2022

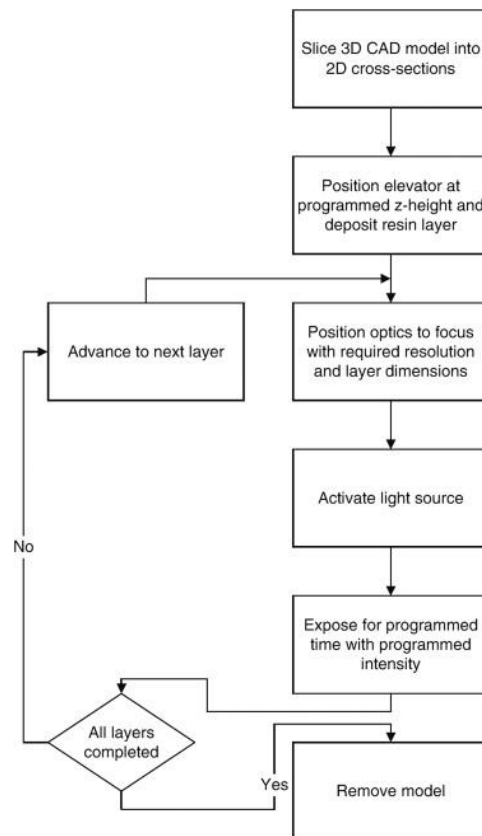


Figure 6. Flowchart of stereolithography. Reproduced from [99] with Elsevier Publishing. Copyright 2017.

2.4. Inkjet.

Inkjet three-dimensional (3D) printing is a quick, versatile, and cost-effective technique that allows the creation of basic and complex 3D items directly from Computer-Aided Design (CAD) data without the use of tooling. Inkjet 3D Printing is a subset of the Solid Freeform Fabrication family of manufacturing processes (SFF) [105]. The layer-by-layer deposition of 3D inkjet printing is comparable to other 3D printing technologies. Printing instructions are created from a 3D mechanical model of the product, exactly like in current fused deposition modeling (FDM) systems. This technique can deposit polymers, dielectric nanoparticles, and conductive nanoparticles, making it applicable to a wide range of materials [106].

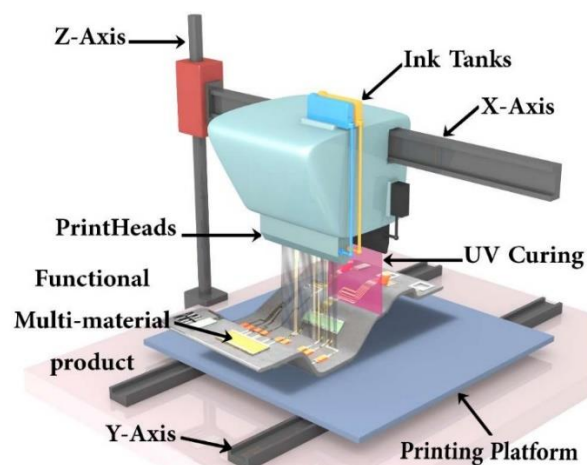


Figure 7. Illustration of inkjet printing. Reproduced from [107] with open access from Polymers—copyright 2022.

This approach uses an effective thermal field under the needle to improve ink viscosity, jetting morphological controllability, and printing structure solidification simultaneously. A steady and finer jet was produced under optimum circumstances, and various 3D structures were directly printed using this jet. Figures 7 and 8 depict illustrations and the mechanism of inkjet printing, while Table 4 shows the utilization of biopolymer.

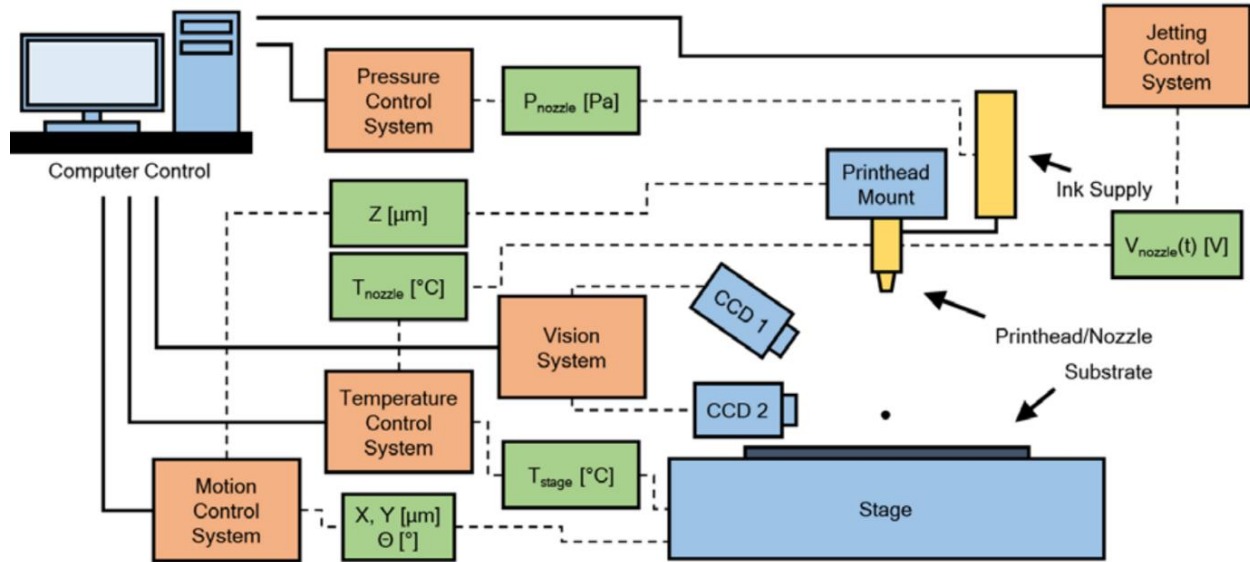


Figure 8. Mechanism of inkjet printing. Reproduced from [108] with open access from Polym. Polym. Compos. Copyright 2022.

Table 4. Overview of Biopolymer Composite Through Inkjet Printing.

Reference	Material	Printing Technique	Mechanical Properties	Application	Year
[109]	SWCNT/Ch	Ink-Jet	N/A	Cardiac Surgery	2021
[110]	PVA/kC	Ink-Jet	Young's Modulus: 10-150MPa	Cartilage Reconstruction	2022
[111]	Algal Polysaccharides	Ink-Jet	N/A	Biomedical Field	2022
[112]	PLA/MBG	Ink-Jet	Compressive Strength: 91.5MPa	Bone Tissue Engineering	2022
[113]	GEIMA/Nanoclay	Ink-Jet	Shear Viscosity: 0.037Pa.s-0.039Pa.s	Sustainable Inks	2020
[114]	Polysaccharides/CaP	Ink-Jet	N/A	Tissue Engineering	2009
[115]	PBAT/SCNP	Ink-Jet	Elastic Modulus: ~45MPa	Biodegradable Product	2017
[116]	PCL/HA/Core-shell	Ink-Jet	Shear Viscosity: ~50Pa.s	Bone Regeneration	2021
[117]	PCL/MWCNT/PEO	Ink-Jet	N/A	Sustainable Material	2018
[118]	Sodium Alginate/CaP	Ink-Jet	Compressive Strength: 0.45-1.0MPa	Bone Tissue Engineering	2022
[119]	PCL/MBG	Ink-Jet	N/A	Bone Tissue Engineering	2022

2.5. Others.

In this review research, some minor printing techniques are non-prominent in AM. Table 5 shows an overview of some minor 3D printing techniques for biopolymer composite. E-jet printing has been used to create different 3D scaffolds with prescribed architecture. E-jet printing is a micro/nano-manufacturing technique that employs an electric field to induce fluid jet printing using micro/nano-scale nozzles [120]. Then, CAWS is a hybrid of AM and wet

spinning that enables fine control of fiber deposition using layer-by-layer technology and the production of an exterior structure or interior architecture [121]. After that, the syringe pump uses bioprinting using the same mechanism layer-by-layer [122]. Direct ink writing (DIW) is the most flexible AM method since it is suited for more materials and may be used to produce complex 3D objects from practically any material, such as ceramic, polymer, metal, or composite (or multi-material) structures. To achieve form fidelity, the ink materials should have high viscoelasticity before extrusion, a good shear-thinning effect when passing through a tiny nozzle, and high viscoelasticity after deposition [123]. Extrudability, form stability, structuration, and interlayer bonding are all buildability criteria for an E3DP building material [124]. Using viscous biopolymer solutions, electrohydrodynamic printing (EHDP) can precisely manipulate the position, size, and morphology of micro-/nano-fibers and fabricate high-resolution scaffolds [125]. In Material Extrusion Additive Manufacturing (MEX), the feedstock containing powder and polymeric binders is heated until the filament softens and can be extruded through a printing nozzle [126].

Table 5. Overview of biopolymer composite through other 3D printing.

Reference	Material	Printing Technique	Mechanical Properties	Application	Year
[127]	PCL/PVP	E-Jet	Thermal Platform: 30°C - 55°C loss	Scaffold	2020
[128]	PHBHHx/PCL	CAWS	Yielding Stress: 0.18-0.36MPa Compressive Strength: 0.16-0.39MPa	3D Porous Scaffold	2017
[129]	PVA/HA/Ch	Syringe pump	Elastic Modulus: 91.14MPa	Hard Tissue Engineering	2019
[130]	PCL/BG	DIW	Compressive Strength: 2.10MPa	Scaffold	2022
[131]	Plant Oil-Based Biopolymer/HA	DIW	Young's Modulus: 11MPa	Biomedical	2019
[132]	BSC	E3DP	Von Mises Yield: $0.435 < \phi < 0.548$	Construction	2021
[133]	PLA/Wood Fibre	MEX	Tensile Strength: 28.4 ± 1.0 MPa	Sustainable Filament	2017
[134]	PCL/Zein	EHDP	Shear Viscosity: 115.6 ± 4.4 Pa.s	Medical	2022

3. Challenges and Future Trends

The utilization of biopolymer composite materials has opened numerous opportunities to develop bio-products in a variety of industries. Only a few studies have been done thus far, even though using biopolymer composites and AM technology can provide enormous flexibility in designing and constructing incredibly complex bioproducts like bone scaffolds. The major reason is the numerous challenges in the biopolymer composite 3D printing process [135]. Firstly, they belong to the category of difficult-to-print materials, and the manufactured products often exhibit severe warpages following the printing process. The other difficulty is that 3D-printed items have poor mechanical qualities, making them unsuitable for applications where material Strength is critical. Advances in material and fabrication technologies that improve the printability of the material will be essential to the future success of 3D printing of biomaterials. Even though many researchers have studied biopolymer composites, it is clear that they have a promising future. Furthermore, the additive manufacturing of biopolymer composite is most commonly utilized in the biomedical area, and due to its high biodegradability, it is predicted to be used more in biomedical devices in the future.

4. Summary

Biopolymer composites offer great features such as biodegradability, biocompatibility, and nontoxicity, making them an ideal choice for biobased components, particularly in manufacturing biomedical equipment. When form complexity and customization are critical considerations, 3D printing technology has opened new doors for future uses of these biomaterials. The current state of 3D printing technology and the applications of additively generated biopolymer composite components in scientific and industrial sectors were evaluated. In summary, the FDM printing method is more common than other printing technologies because of the widespread availability of low-cost equipment and ease of processing. As a result, extensive research is required to assess and enhance the processability and final performance.

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Conflicts of Interest

The authors declare no conflict of interest.

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